A Region-of-Interest Approach for Detecting Progression of Glaucomatous Damage With Optical Coherence Tomography

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IMPORTANCE Detecting progression of glaucomatous damage is often challenging.

OBJECTIVE To test the feasibility of using frequency-domain optical coherence tomography (FD-OCT) and a region-of-interest (ROI) approach to measure progressive changes in glaucomatous damage.

DESIGN, SETTING, AND PARTICIPANTS Among a group of patients in an institutional glaucoma practice who were likely to show glaucoma progression, eyes with a history of an optic disc hemorrhage (DH) confirmed by stereophotography were followed up with FD-OCT cube scans of the optic disc. All patients underwent FD-OCT scans on at least 2 occasions separated by at least 1 year (mean, 3.45 years; range, 1.42-6.39 years). Because we were not studying the effects of an optic DH, no constraint was placed on the time between the documentation of an optic DH and the first scan used in the analysis.

MAIN OUTCOMES AND MEASURES After en face images of the FD-OCT scan were aligned based on the blood vessels, circumpapillary images were derived for an annulus 100 μm in width, and the retinal nerve fiber layer (RNFL) thickness profiles were plotted for the first and last visits. The ROI width associated with the optic DH was defined as the region of the RNFL profile below the 1% CI based on healthy norms. The change in the ROI width was compared with the change in the global RNFL thickness, which was obtained by averaging the circumpapillary RNFL thickness.

RESULTS The change in the ROI width (mean [SD], 8.0° [6.4°]; 95% CI, 4.9° to 11.1°; range, −0.7° to 19.3°) was significant (P < .001, 2-tailed t test) while the change in the global thickness (mean [SD], 2.40 [5.87] μm; 95% CI, −0.48 to 5.28 μm) was not significant (P > .12, 2-tailed t test). Although 15 of the 16 ROIs increased in width between visits, only 11 showed a decrease in the global RNFL thickness.

CONCLUSIONS AND RELEVANCE For detecting progression of local RNFL damage in patients with glaucoma, an OCT ROI approach appears superior to the OCT global RNFL thickness measure typically used.

Published online October 22, 2015. Corrected on March 10, 2016.
Detecting progression of glaucomatous damage presents a challenge to the physician. Although various approaches have been proposed based on optical coherence tomography (OCT), 2 recent reviews favored retinal nerve fiber layer (RNFL) thickness measures of optic disc scans. However, while the authors of one study preferred measuring changes in the global (mean) RNFL thickness of a circumpapillary region, authors of the other study argued for analyzing the RNFL thickness maps of the entire region around the disc.

Our approach also measures the RNFL thickness from optic disc scans. However, unlike the global RNFL thickness of circumpapillary scans, we examine the change in a local circumpapillary region of interest (ROI). Although this approach is comparable to the event analysis of serial RNFL thickness maps, it is based on a different principle. In particular, our ROI method is part of a general strategy that analyzes OCT scans in a way similar to that used by a radiologist when analyzing a magnetic resonance imaging or computed axial tomography scan.

To assess the usefulness of this ROI approach, we examined eyes with an optic disc hemorrhage (DH). The objective herein was not to study the effects of optic DH but rather to study a group of eyes known to be prone to glaucoma progression. In particular, we measured the change in the width of the abnormal region of an RNFL thickness near the site of an earlier optic DH. To assure that the same region was studied over time, the OCT scans were aligned based on the location of the blood vessels.

Methods

Study procedures followed the tenets of the Declaration of Helsinki, and the protocol was approved by the institutional review boards of Columbia University and the New York Eye and Ear Infirmary of Mount Sinai. Patients were selected from an ongoing prospective early glaucoma study between the 2 institutions. Written informed consent was obtained from all participants, and the protocol adhered to the tenets of the Declaration of Helsinki.

Participants

Sixteen eyes from 16 patients with glaucoma (mean [SD] age, 56.8 [10.6] years) with an optic DH confirmed on stereophotography and with refractive error within ±6 diopters were included in the study. For each patient, the Table summarizes the diagnosis and the mean deviation of 24-2 Humphrey visual fields. As expected, most eyes (13 of 16) had an optic DH in the inferotemporal region of the disc. All eyes underwent frequency-domain OCT (FD-OCT) cube scans of the optic disc (3D OCT-1000; Topcon) obtained on at least 2 occasions separated by at least 1 year (mean, 3.45 years; range, 1.42-6.39 years). Both scans had to occur after the appearance of an optic DH on stereophotography. An optic DH was defined as a splinter-like or flame-shaped hemorrhage on or within the RNFL or neuroretinal rim, as identified by a glaucoma specialist (R.R.). The appearance of an optic DH was used to identify a region that would likely show glaucoma progression. Because we were not studying the effects of an optic DH, no constraint was placed on the time between the documentation of an optic DH and the first scan used in the analysis, which was obtained 3 days to 8.3 years (median, 78 days) after the identification of an optic DH.

### ROI Approach

The borders of the RNFL were determined with a commercial software program (SSV; Topcon). If needed, the borders were then manually corrected by one of us (D.W.) masked to the study objective and chronological sequence of the scans.

For each eye, en face images of the first and last disc cube scans (6 × 6 mm, 3D OCT-2000; Topcon) were registered by centering both scans on the optic disc center and then rotating to align the blood vessels. After the alignment, circumpapillary images (Figure 1A) were created for each eye and the RNFL thickness profiles (Figure 1B) were plotted for the first (dashed lines) and last or most recent (solid lines) visits. The RNFL profiles are shown with the temporal quadrant in the center, where 0° corresponds to the 9-o’clock position (right eye) and the 3-o’clock position (left eye).

### Table. Patient Diagnoses and Visual Field Mean Deviation Values

<table>
<thead>
<tr>
<th>Patient No.</th>
<th>Eye</th>
<th>Diagnosis</th>
<th>First Visit</th>
<th>Last Visit</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>Left</td>
<td>PG</td>
<td>−8.28</td>
<td>−13.18</td>
</tr>
<tr>
<td>2</td>
<td>Right</td>
<td>POAG</td>
<td>−0.88</td>
<td>−2.28</td>
</tr>
<tr>
<td>3</td>
<td>Right</td>
<td>XFG</td>
<td>0.64</td>
<td>0.44</td>
</tr>
<tr>
<td>4</td>
<td>Right</td>
<td>POAG</td>
<td>−8.71</td>
<td>−16.31</td>
</tr>
<tr>
<td>5</td>
<td>Right</td>
<td>POAG</td>
<td>−8.41</td>
<td>−8.79</td>
</tr>
<tr>
<td>6</td>
<td>Left</td>
<td>POAG</td>
<td>−1.59</td>
<td>−1.67</td>
</tr>
<tr>
<td>7</td>
<td>Right</td>
<td>POAG</td>
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<td>−1.98</td>
</tr>
<tr>
<td>8</td>
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<td>POAG</td>
<td>−1.83</td>
<td>−2.39</td>
</tr>
<tr>
<td>9</td>
<td>Right</td>
<td>POAG</td>
<td>−0.05</td>
<td>−1.11</td>
</tr>
<tr>
<td>10</td>
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<td>POAG</td>
<td>−5.45</td>
<td>−7.95</td>
</tr>
<tr>
<td>11</td>
<td>Right</td>
<td>POAG</td>
<td>−3.01</td>
<td>−7.71</td>
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<tr>
<td>12</td>
<td>Right</td>
<td>POAG</td>
<td>−15.39</td>
<td>−15.32</td>
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<tr>
<td>13</td>
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<td>POAG</td>
<td>−1.12</td>
<td>−1.04</td>
</tr>
<tr>
<td>14</td>
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<td>POAG</td>
<td>−6.85</td>
<td>−10.17</td>
</tr>
<tr>
<td>15</td>
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<td>POAG</td>
<td>−7.75</td>
<td>−9.32</td>
</tr>
<tr>
<td>16</td>
<td>Left</td>
<td>POAG</td>
<td>−2.85</td>
<td>−3.58</td>
</tr>
</tbody>
</table>

Abbreviations: PG, pigmentary glaucoma; POAG, primary open-angle glaucoma; XFG, exfoliation glaucoma.
The abnormal region closest to the optic DH was considered the ROI. This approach was used based on the knowledge that glaucoma progression usually occurs because of the development of a new defect or the expansion of a preexisting one (or a combination of both). The width of this ROI was defined as the portion of the scan below the 1% CI based on healthy norms (red region in Figure 1B). The widths (in degrees) of the ROI (blue and red horizontal bars in Figure 1A) for the first and last visits were obtained. A custom software program (MATLAB; MathWorks) determined the alignment of the images, the definition of the ROI, and the ROI width.

Results

Three of the 16 ROIs were in the superior half of the disc, and 13 were in the inferior half. The blue and red horizontal bars in Figure 2 show the locations and widths of the abnormal ROIs for the first (blue) and last (red) visits. The 13 ROIs in the lower half of the disc were in the inferior portion of the temporal quadrant and the temporal portion of the inferior quadrant. The 3 ROIs in the upper half of the disc were in the temporal half of the superior quadrant. In 14 eyes, the region of the disc affected included the portion of the disc associated with the macula (±8° of central vision).12-14

Fifteen of the 16 ROIs increased in width between visits, and 1 ROI (patient 3 in the Table) decreased by less than 1°. The ROI widths varied from 7.4° to 61.4° (mean [SD], 24.8° [14.3°]) for the first visit and from 19.0° to 68.1° (mean [SD], 32.8° [16.3°]) for the last visit. The ROI width changed by a mean (SD) of 8.0° (6.4°) (95% CI, 4.9° to 11.1°) (range, −0.7° to 19.3°). This increase was significant (P < .001, 2-tailed t test).

In contrast, the global thickness decreased by a mean (SD) of 2.40 (5.87) μm (95% CI, −0.48 to 5.28 μm), which was not significant (P > .12, 2-tailed t test). In addition, fewer eyes (11 of the 16) showed a decrease in the global RNFL thickness.
All eyes underwent a second OCT imaging session on day 1 of testing. These scans can be used to obtain a sense of whether the change for an individual eye is statistically reliable. The ROI width of 8 of 16 eyes exceeded the 2-tailed 95% CI based on the results of the second scans, which showed a mean (SD) width of −0.04° (3.78°), while the ROI width in none of the eyes was less than the 2-tailed 95% CI. In contrast, the global RNFL thickness of 3 eyes was less than the 2-tailed 95% CI based on the results of the second scans, which demonstrated a mean (SD) of 0.11 (2.61) μm, although the global thickness of 1 eye was thicker than the 2-tailed 95% CI.

Discussion

While the global (mean) RNFL thickness is a commonly used OCT measure for assessing glaucoma progression, we hypothesized that an ROI approach would be superior for assessing progression of local damage. The results herein support this hypothesis. There are 2 possible reasons why this approach has not been widely used.

The first concerns the placement of the circle used to derive the RNFL thickness plot. If circle scans are used, they will not necessarily be in the same location for the earlier and later scans unless the OCT imaging system has eye-tracking capability. When cube scans are used to derive a circumpapillary RNFL thickness, as in this study, the alignment can still be off because of torsion of the eye or failure to correctly identify the same center of the eye. Herein, we overcame this problem by registering the images so that the blood vessels were aligned.

The second concerns the nature of glaucomatous damage, which can be diffuse and local, even in the macula and early in the disease process. In cases of purely diffuse damage, a global measure may be more suitable. However, diffuse damage is often accompanied by local damage, and an ROI approach is useful in these patients.
The RNFL thickness change map that is a capability of the imaging system’s glaucoma progression analysis (CIRRUS; Carl Zeiss Meditec) allows for assessing local changes in the RNFL thickness. However, our approach has the advantage of providing a single metric of progression of damage. In addition, it encourages direct viewing of the scan. The OCT scans have better spatial resolution than the magnetic resonance imaging or computed axial tomography scans, but many glaucoma specialists focus on the summary statistics instead of the scan itself. Hood and Raza have argued that the circumpapillary scan should be viewed directly for 2 reasons. First, it allows the physician to assess if the borders of the RNFL have been correctly identified (segmented) by the automated algorithm. Second, it allows for direct visualization of local damage missed by other
methods. However, our approach has the disadvantage of examining only one location, a circle with a 3.45-mm diameter. Leung et al. provided evidence that a 4-mm diameter would be better for detecting progression of damage. In addition, the ROI analysis could be applied to derived circle scans of different widths.

Our study had several limitations. It was designed to provide a proof of concept for an ROI approach as opposed to the global RNFL thickness. However, to obtain a better measure of the relative accuracy of the 2 methods, more work is needed. In particular, the sensitivity and specificity of a larger group of patients should be measured using an event-based approach with second measures on different days or a trend-based approach in which eyes are followed up with more frequent tests and perhaps for a longer period.

In addition, we only included regions and eyes with a history of an optic DH. Although this limitation was convenient for a proof-of-concept study, a larger sample should include eyes without a history of an optic DH, which raises the question of how to define an ROI in these eyes. As in the present study, we suggest defining an ROI as the portion of the scan below the 1% CI based on healthy norms. However, instead of restricting the ROI to the region near an optic DH, we suggest defining it as any region beyond a certain criterion width and perhaps depth. For comparison with visual fields, it might be useful to also restrict the ROI to the temporal half of the disc. More work is needed to optimize the criteria for the width or depth of the ROI. We avoided using depth as a criterion because many of the defects had already reached a minimum RNFL thickness. However, the area within the abnormal region (red in Figure 1B) should be explored as a possible alternative to the width of this region. Our ultimate goals are to automate the definition of the ROI on baseline scans and to provide the physician with an indication of the change in the ROI on subsequent visits.

Other methods that use more of the information in the disc cube scan (eg, the glaucoma progression analysis) should be compared with the ROI method. Our bias herein was to include an en face analysis in future studies. In collaboration with Fortune et al. and using specialized software they developed, Hood et al. recently showed that an en face slab analysis of swept-source OCT can reveal details of glaucomatous damage not visible on the RNFL thickness plots. In the Hood et al study, en face images based on the mean reflectance intensity were generated from 52-μm slabs just below the vitreous border of the inner limiting membrane. To illustrate this en face slab technique, we examined data for patient 4 in the Table, an eye for which we had swept-source OCT scans for both the first and last visits. Figure 3A shows the FD-OCT RNFL profiles for this eye in the same format as in Figure 1B. The en face slab image based on the swept-source OCT scan from the first visit is shown in Figure 3B. Figure 3C (left) shows an enlargement of the region within the red square in Figure 3B, and Figure 3C (right) shows the same region for the last visit. The tips of the green arrowheads indicate the same locations in all panels. The small increase in width seen in Figure 3A corresponds to the change in contrast seen in the regions just to the left of the blood vessels (green arrowheads). These changes are easier to see in the locations farther from the disc, such as the regions indicated by the white arrows, which are in the same locations. While these results are preliminary, they support the suggestion that an en face slab analysis may be clinically useful.

Conclusion

For detecting progression of local RNFL damage in patients with glaucoma, an OCT ROI appears superior to the OCT global RNFL thickness measure typically used.

REFERENCES


8. De Moraes CG, Demirel S, Gardiner SK, et al. Rate of visual field progression in eyes with optic